

# **Microactuators and Sensors for Microfluidics and Lab on a Chip applications**

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and SRC

Slides 20-56 are contributed by Michael Ramsey (Oak Ridge)

General reference: Nanoelectromechanics in Engineering and Biology, by M. P. Hughes

# Current Status of Electronics

- The current status of the integrated circuits
  - Device size ~ 10 nm
  - Integration Level ~  $10^9$ /chip
  - Power ~ 100 W                      Leakage ~ 20 W
  - Other features: Power Supply ~ 1.5 V

# Intelligent Silicon

Nano is Here

New **Devices**,  
**Materials**, and **Processes**

Expanding the Silicon Canvas

EXTENDING MOORE'S LAW

Discrete

SSI

LSI

VLSI

**Nano**



Silicon Innovation Enabling Convergence

Sensors

Optical

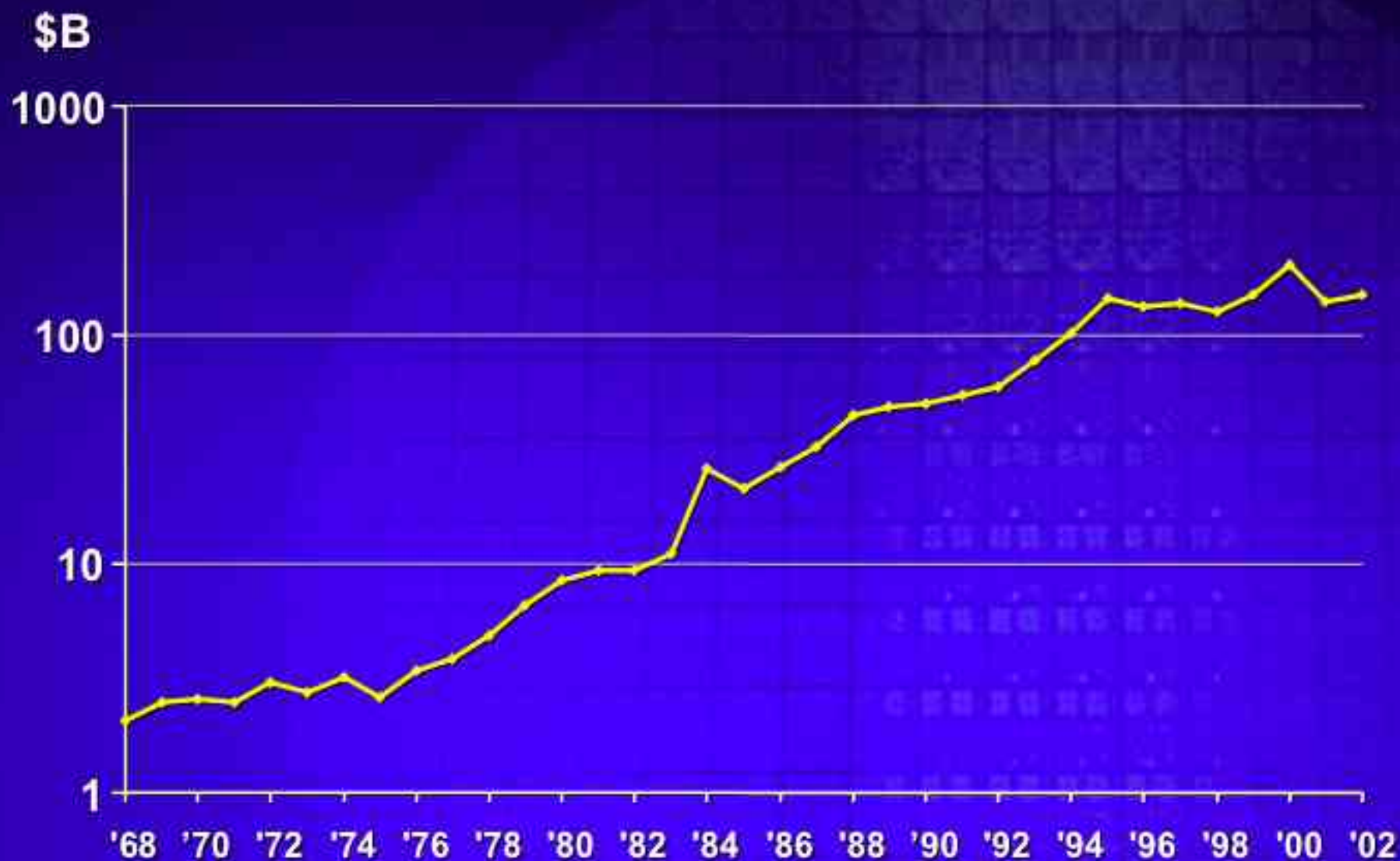
Wireless

Mechanical

EXPANDING

MEMS/NEMS  
Microfluidics  
Lab-on-a-chip

# Worldwide Semiconductor Revenues



# Average Transistor Price By Year



# Integrated Circuit Complexity

Transistors

Per Die

$10^{10}$

$10^9$

$10^8$

$10^7$

$10^6$

$10^5$

$10^4$

$10^3$

$10^2$

$10^1$

$10^0$

◆ 1965 Actual Data

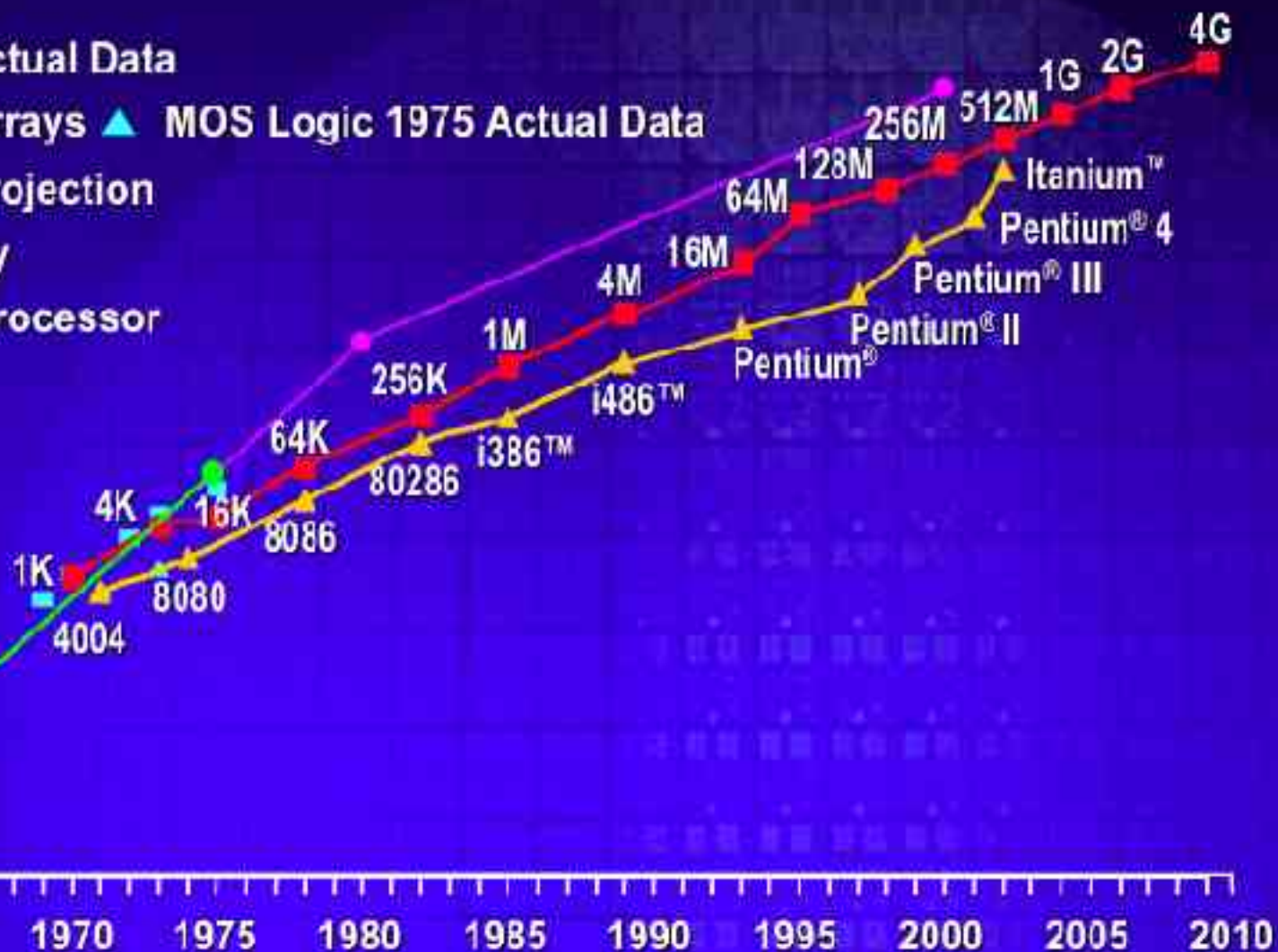
■ MOS Arrays ▲ MOS Logic 1975 Actual Data

● 1975 Projection

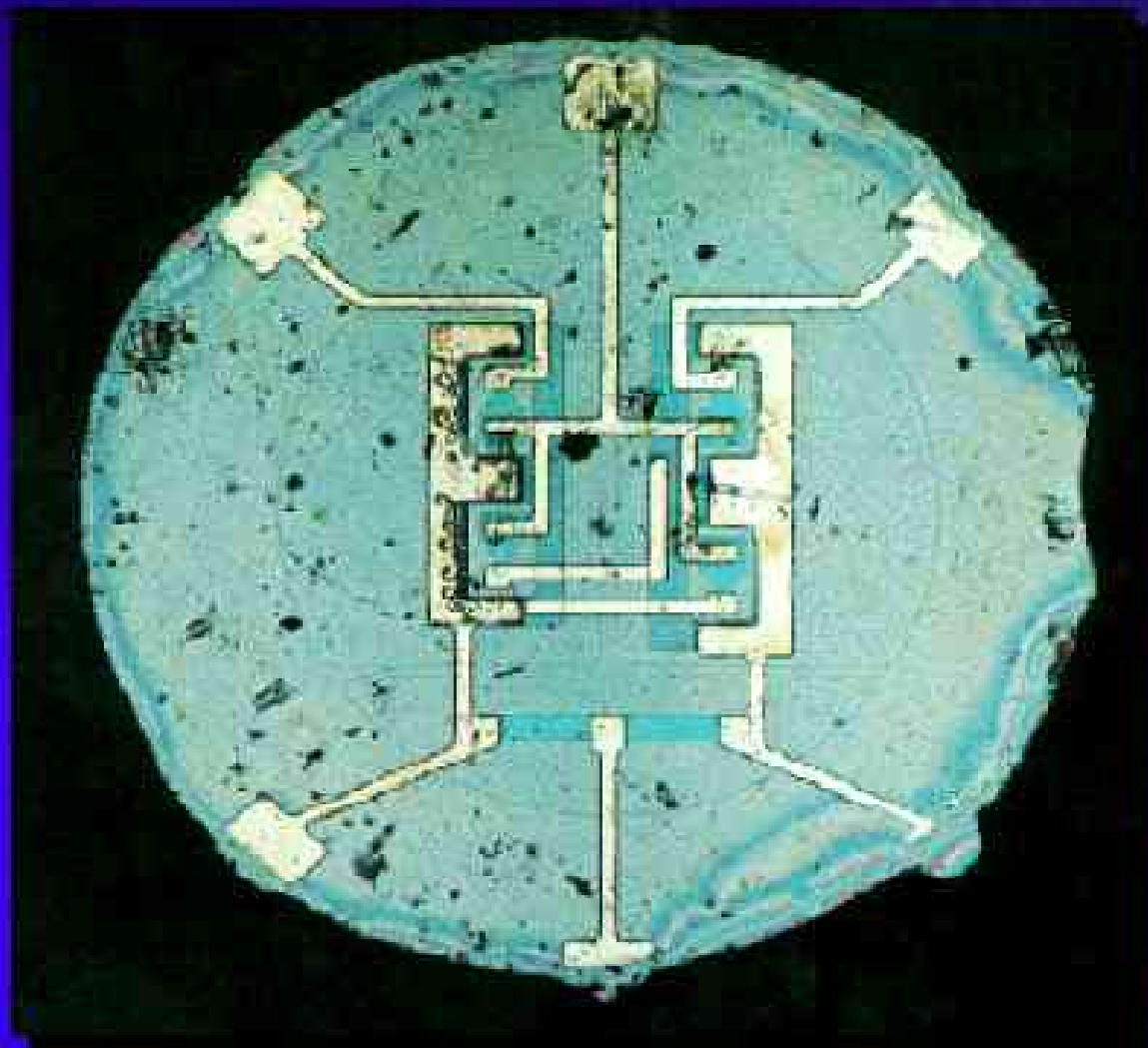
■ Memory

▲ Microprocessor

1960 1965 1970 1975 1980 1985 1990 1995 2000 2005 2010



# The First Planar Integrated Circuit, 1961



# 1 $\mu\text{m}^2$ SRAM Cell

P501 Contact  
1978

P1262 SRAM Cell  
2002

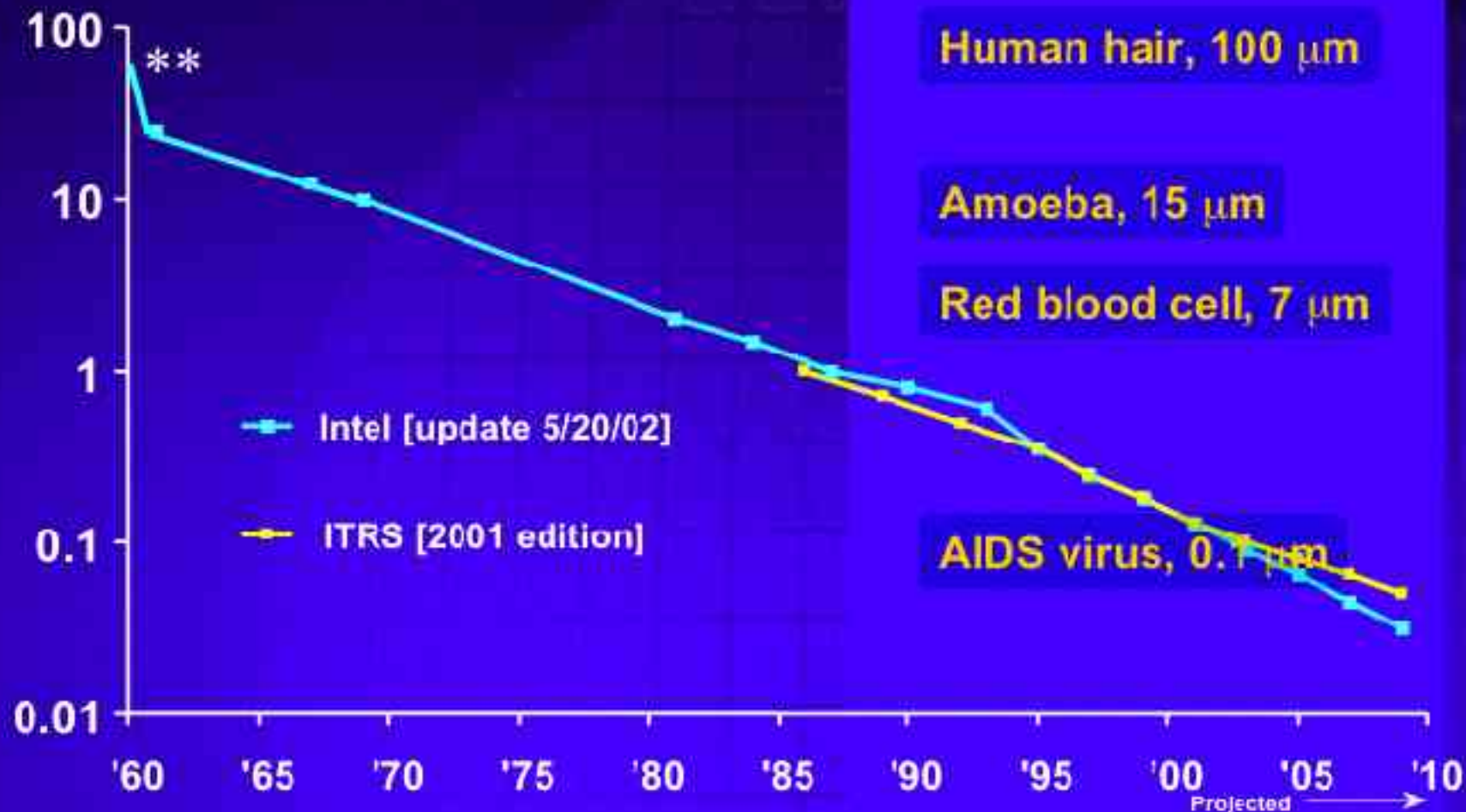


1  $\mu\text{m}$



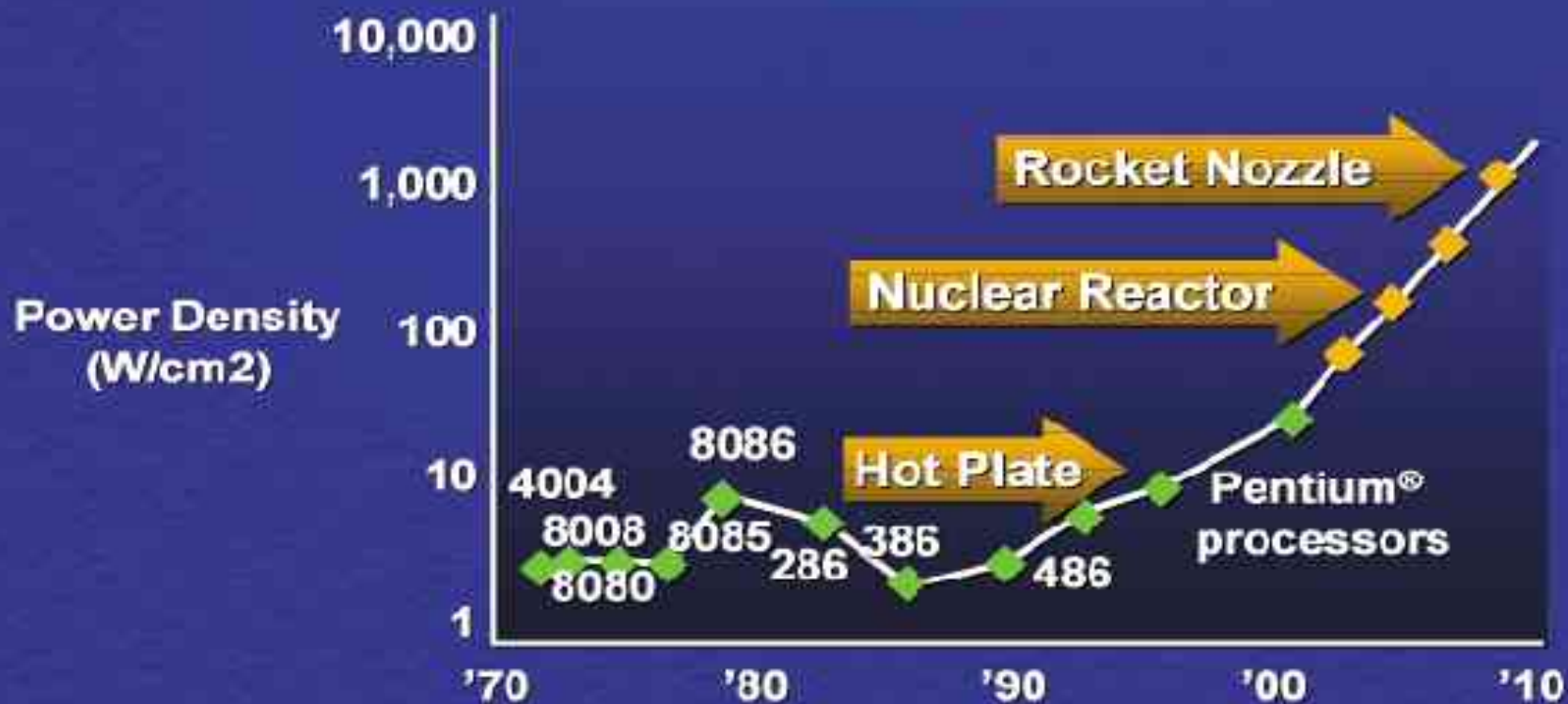
# Minimum Feature Size

Feature Size  
(microns)



\*\* Planar Transistor; remaining data points are ICs.  
Source: Intel, post '96 trend data provided by SIA  
International Technology Roadmap for Semiconductors (ITRS)  
^ [ITRS DRAM Half-Pitch vs. Intel "Lithography"]

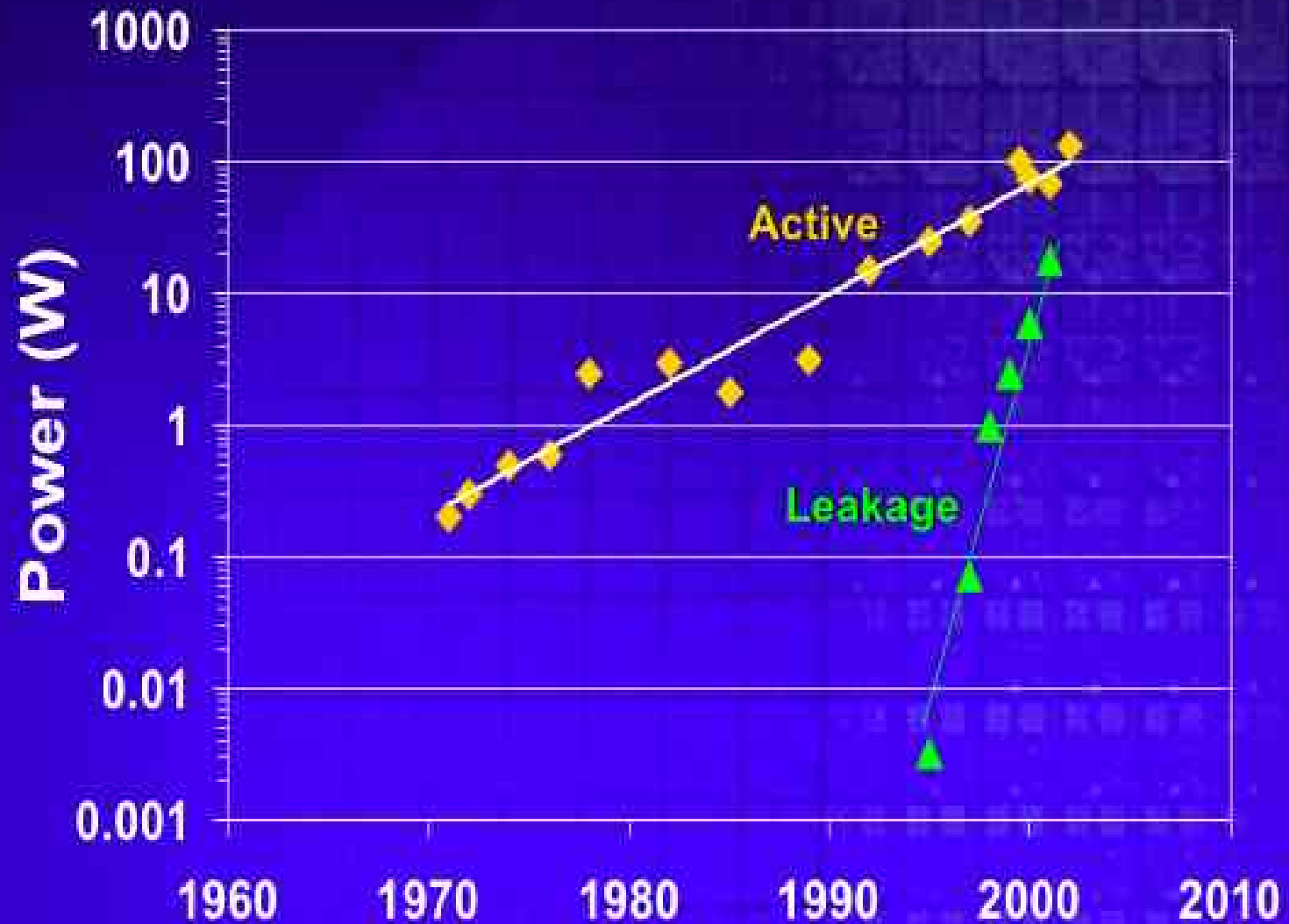
# Power Density Will Get Even Worse



## Need to Keep the Junctions Cool

- Performance (Higher Frequency)
- Lower leakage (Exponential)
- Better reliability (Exponential)

# Processor Power (Watts) - Active & Leakage



# New Materials, Devices Extend Si Scaling

## Changes Made

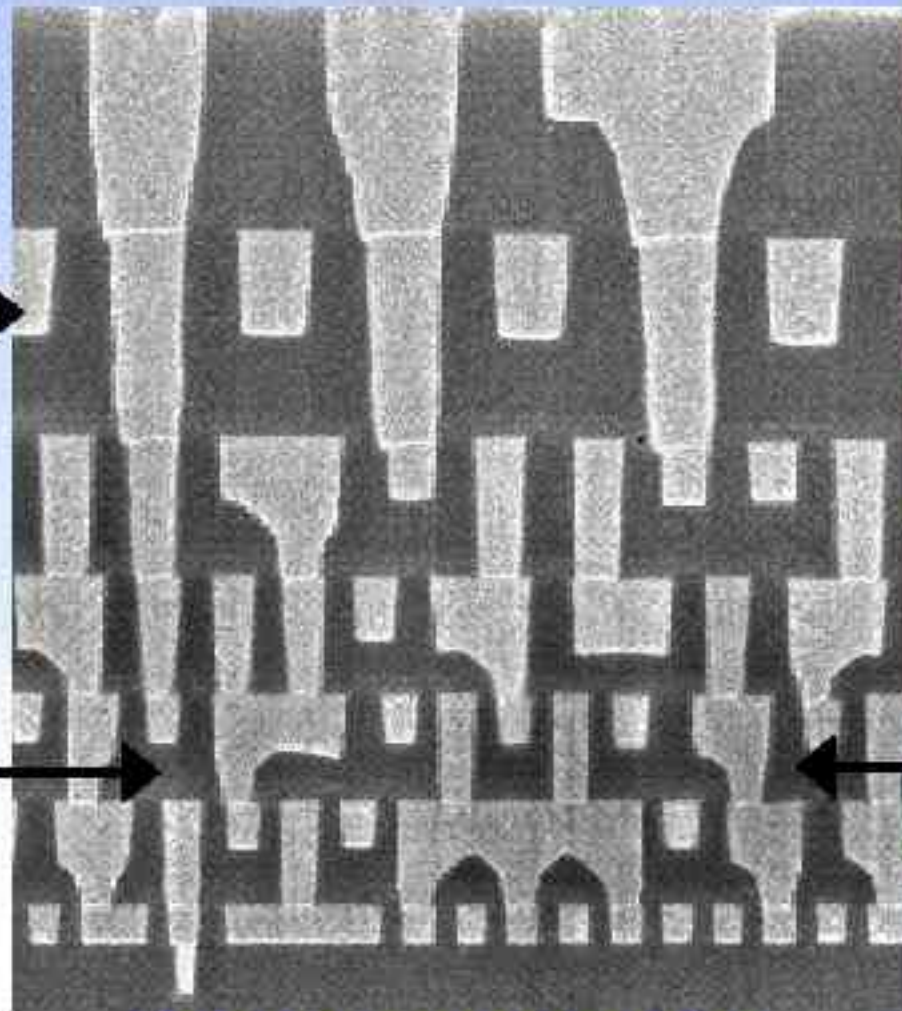
**Metal lines**

Al  $\rightarrow$  Cu

**Insulating dielectric**

SiO<sub>2</sub>  $\rightarrow$  SiOF

$\rightarrow$  CDO  
(low-k)



## Future Options

Ultra  
Low-k  
Dielectric

**Interconnects**

Source: Intel

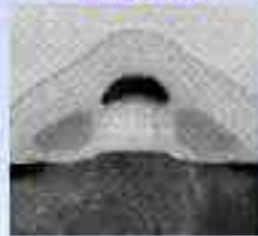
# Intel Nano Transistors

90nm Node  
2003



50nm Length  
(IEDM2002)

65nm Node  
2005



30nm Prototype  
(IEDM2000)

45nm Node  
2007



20nm Prototype  
(VLSI2001)

32nm Node  
2009



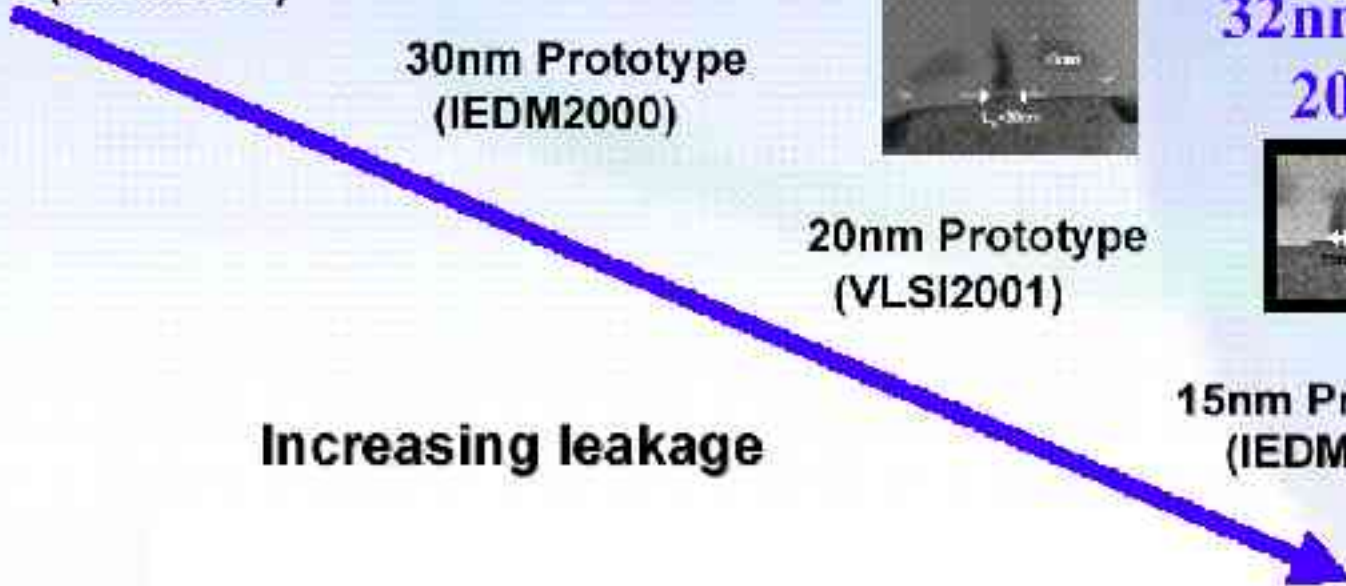
15nm Prototype  
(IEDM2001)

22nm Node  
2011

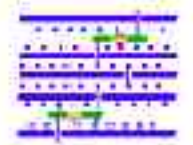
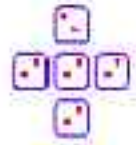
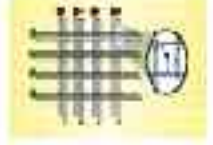
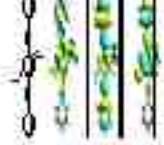
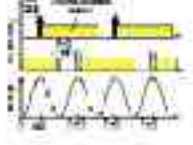



10nm Prototype  
(ITJ 2002)

Increasing leakage



# Emerging Research Architectures

ARCHITECTURE	 <b>3-D INTEGRATION</b>	 <b>QUANTUM CELLULAR AUTOMATA</b>	 <b>DEFECT TOLERANT ARCHITECTURE</b>	 <b>MOLECULAR ARCHITECTURE</b>	 <b>CELLULAR NONLINEAR NETWORKS</b>	 <b>QUANTUM COMPUTING</b>
<b>DEVICE IMPLEMENTATION</b>	CMOS with dissimilar material systems	Arrays of quantum dots	Intelligently assembled nanodevices	Molecular switches and memories	Single electron array architectures	Spin transistors, NMR devices, Single flux quantum devices
<b>ADVANTAGES</b>	Less interconnect delay. Enables mixed technology solutions	High functional density. No interconnects in signal path	Supports hardware with defect densities ~50%	Supports memory based computing	Enables utilization of single electron devices at room temperature	Exponential performance scaling, Enables unbreakable cryptography
<b>CHALLENGES</b>	Heat removal, No design tools, Difficult test and measurement	Limited fan out, Dimensional control (low temperature operation), Sensitive to background charge	Requires pre-computing test	Limited functionality	Subject to background noise, Light tolerances	Extreme application limitation, Extreme technology
<b>MATURITY</b>	Demonstration	Demonstration	Demonstration	Concept	Demonstration	Concept

~2009?



2015++



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Lab-on-a-chip

# Microfabricated Chemical Measurement Systems

- Lab-on-a-Chip
  - Microfabricated fluidic circuits for chemical analysis
- Nanofluidics
- Micro Ion Trap Mass Spectrometry
- Micro Ion Mobility Spectrometry



# **Lab-on-a-Chip: Objectives**

- **Integrate multiple steps of a measurement or synthesis protocol into a microfabricated fluidic device**
- **Utilize existing laboratory principles taking advantage of scaling where possible**
- **Design devices that can be mass produced**

# Lab-on-a-Chip: Benefits

- **Automation**
- **Reagent consumption reduced  $10^4$  -  $10^6$**
- **Speed -  $10^2$**
- **High quality data**
- **Scale up at low cost**
- **Inexpensive/disposable devices (chips)**
- **Standardized platforms**
- **CAD/A - Rapid prototyping**

# Applications

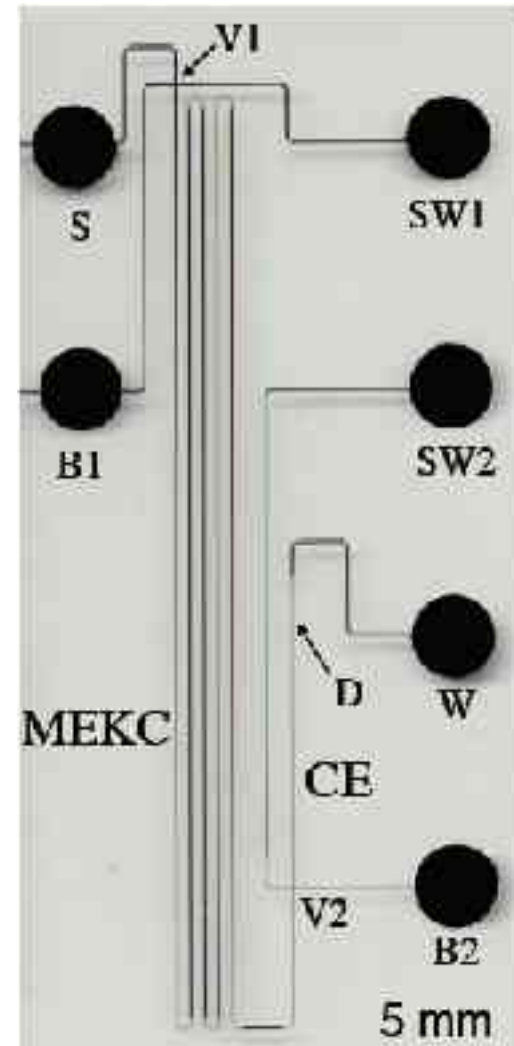
- **In-situ Measurements**
  - Process Control
  - Environmental Monitoring
- **Field Analysis**
  - Environmental Monitoring
  - Forensics
- **Medical Diagnostics**
  - Point-of-Care
  - Emergency Care
  - Closed-Loop Monitoring/Dosing
- **High-throughput Laboratory Analysis**
  - Combinatorial Discovery
  - DNA Sequencing
  - Proteomics

# Synthesis Applications

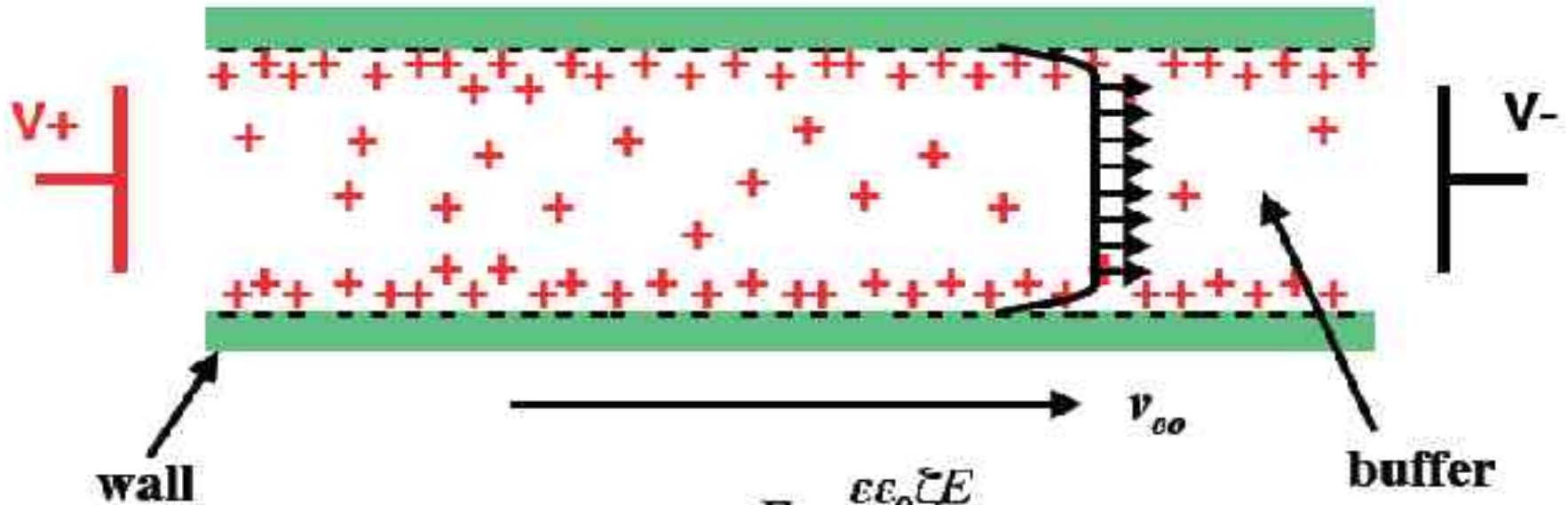
- Materials Discovery
  - Vaccines
  - Coatings
  - Electronics
- Just in time production
  - Hazardous materials
- Production development/optimization
  - Pharmaceuticals
  - Materials

# Microfluidic Devices

- Materials
  - Silica (and other silicon related)
  - Plastics (polymers)
- Dimensions (channels)
  - 20-100  $\mu\text{m}$  wide
  - 0.05-30  $\mu\text{m}$  deep
  - 1-20  $\text{cm}^2$  substrates
- Volumes
  - 1 fL - 1 nL manipulations
  - 1-100  $\mu\text{L}$  reservoirs
- Fluid transport
  - electrokinetic
  - pressure
  - surface tension



# Electrokinetic Transport



$$v_{eo} = \mu_{eo} E = \frac{\epsilon \epsilon_0 \zeta E}{4\pi r \eta}$$

$$v_{ep} = \mu_{ep} E = \frac{ezE}{6\pi r \eta}$$

$$v_{eff} = \mu_{eff} E = (\mu_{eo} + \mu_{ep}) E$$

eo: electroosmosis

ep: electrophoresis

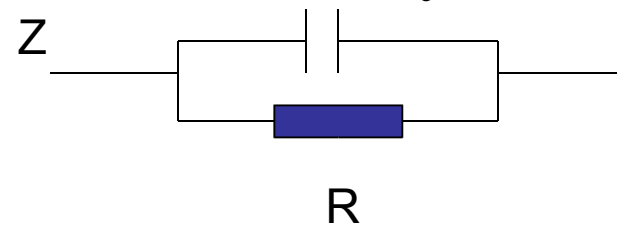
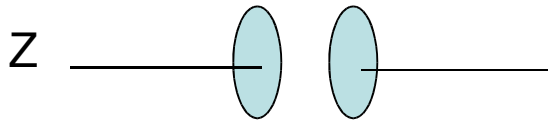
$\eta$ : viscosity

# Electrokinetic Forces

Force	AC or DC	Origin ( <b>Force</b> )
Electrophoresis	DC	Caused by charge in E-field ( <b>QE</b> )
Dielectrophoresis (DEP)	AC/DC	Caused by induced dipole in field gradient ( <b>Qd. <math>\nabla E</math></b> )
Electro-osmosis	AC/DC	Caused by interaction between double layer charges and tangential E-field
Electrorotation	AC	Caused by dipole lag in rotating E-field ( <b>Torque=Dd X E</b> )
Traveling wave DEP	AC	Caused by dipole lag in traveling E-field
Electro-orientation	AC/DC	Caused by interaction between dipole and electric field

# Polarization, Relaxation and Dispersion

- $Z^{-1} = R^{-1} + X_c$  Resistance:  $R = d / \sigma A$
- Reactance:  $X_c = 1 / \omega C$
- $C = \epsilon^* A / d$
- $\epsilon^* = \epsilon_0 \epsilon_r - j \sigma / \omega$  ↗ Includes both dielectric and conductivity effects



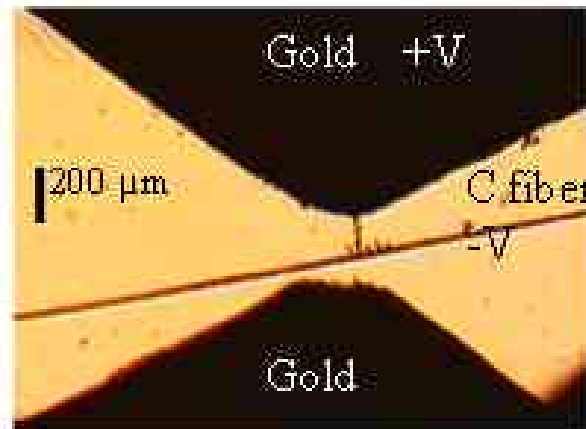
$\omega \ll 0$   $\sigma$  dominates,  $\omega \ll 8$   $\epsilon_r$  dominates in between there is a transition dispersion



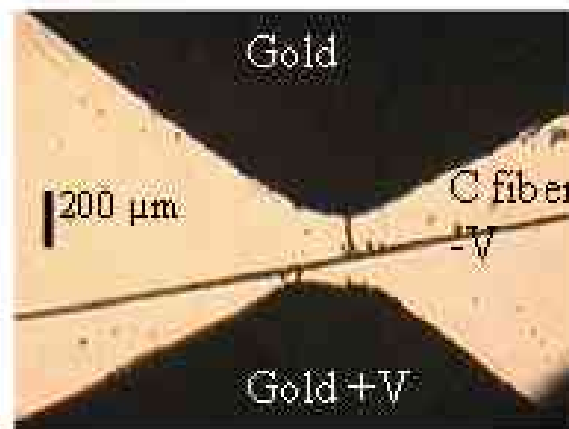
# Dispersions

- Internal dispersion:
  - Debye relaxation
- Dispersion at the interface between two different materials:
  - Maxwell-Wagner relaxation
- These and other dispersions results in frequency dependence of forces on nanoparticles

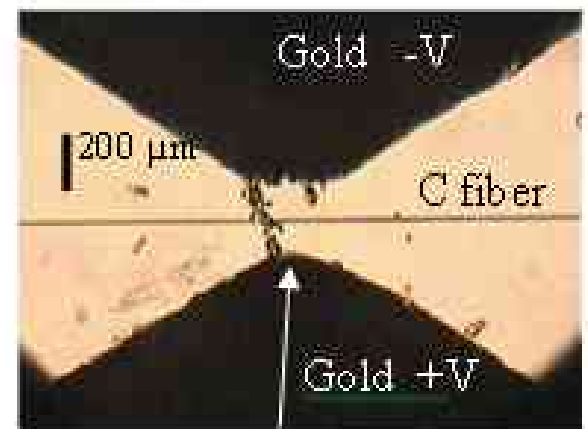
# Dielectrophoresis/Electrophoresis



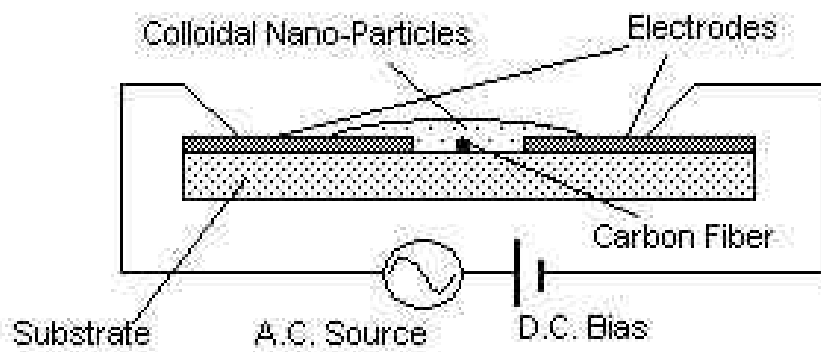
(a)



(b)



(c)

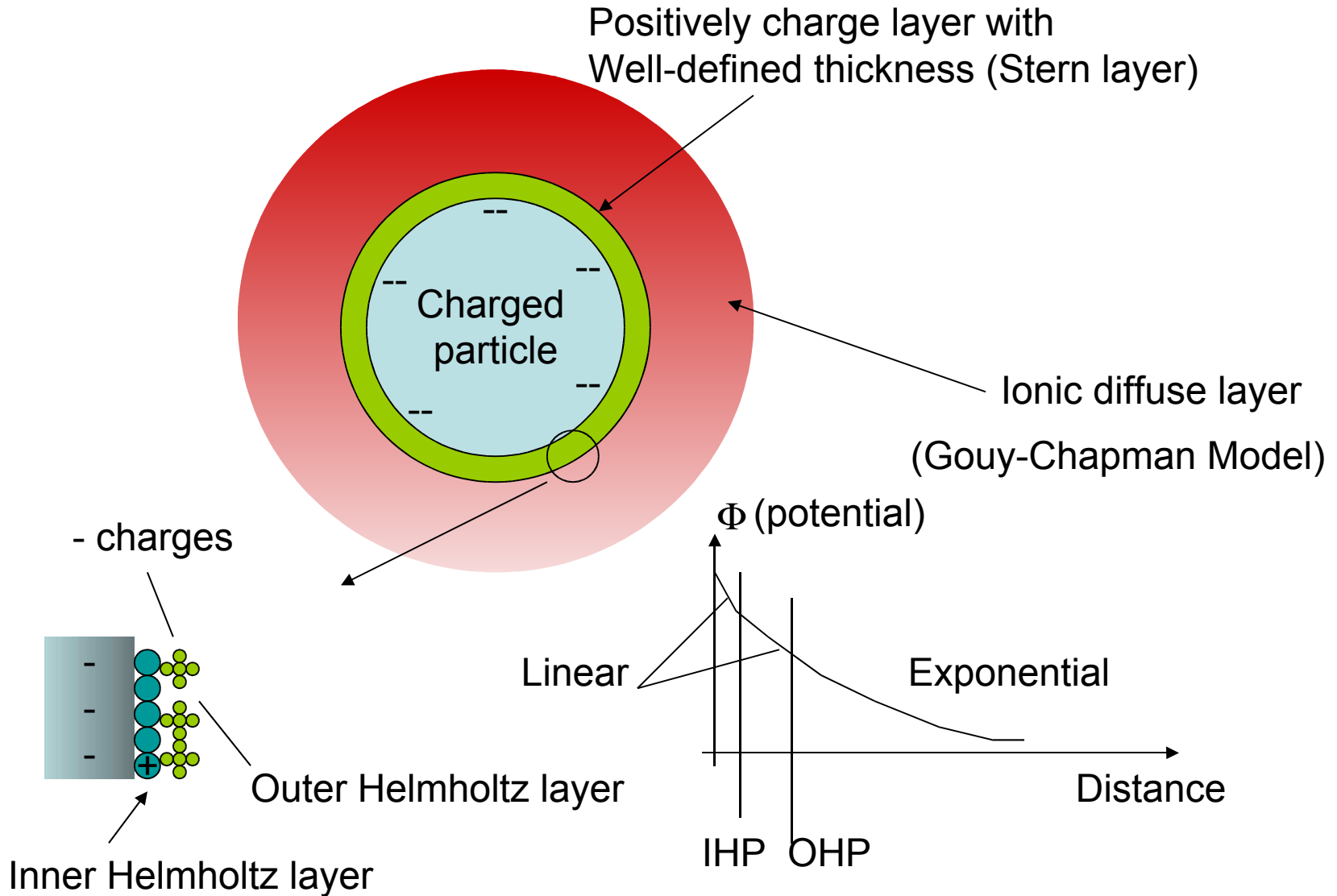


(d)

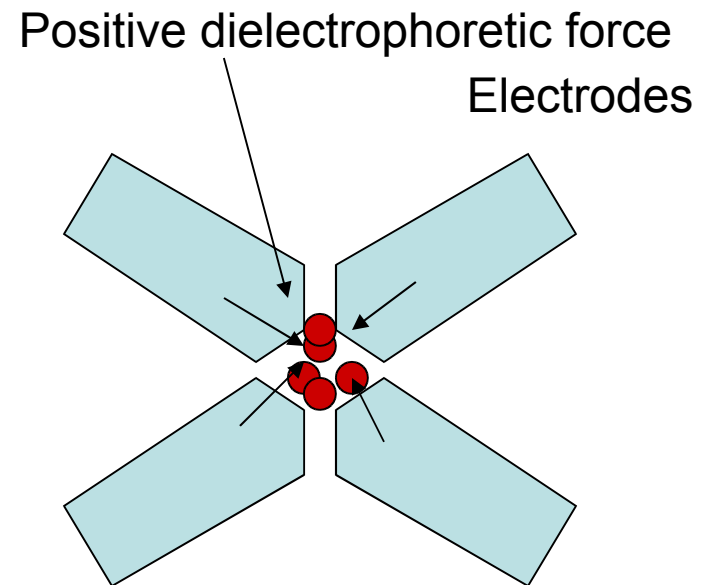
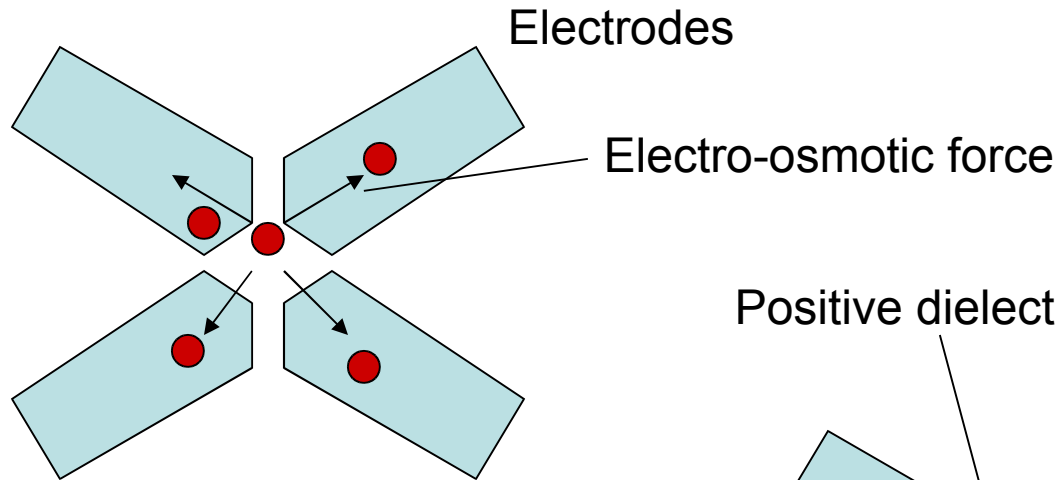


(e)

# Electric Double Layer

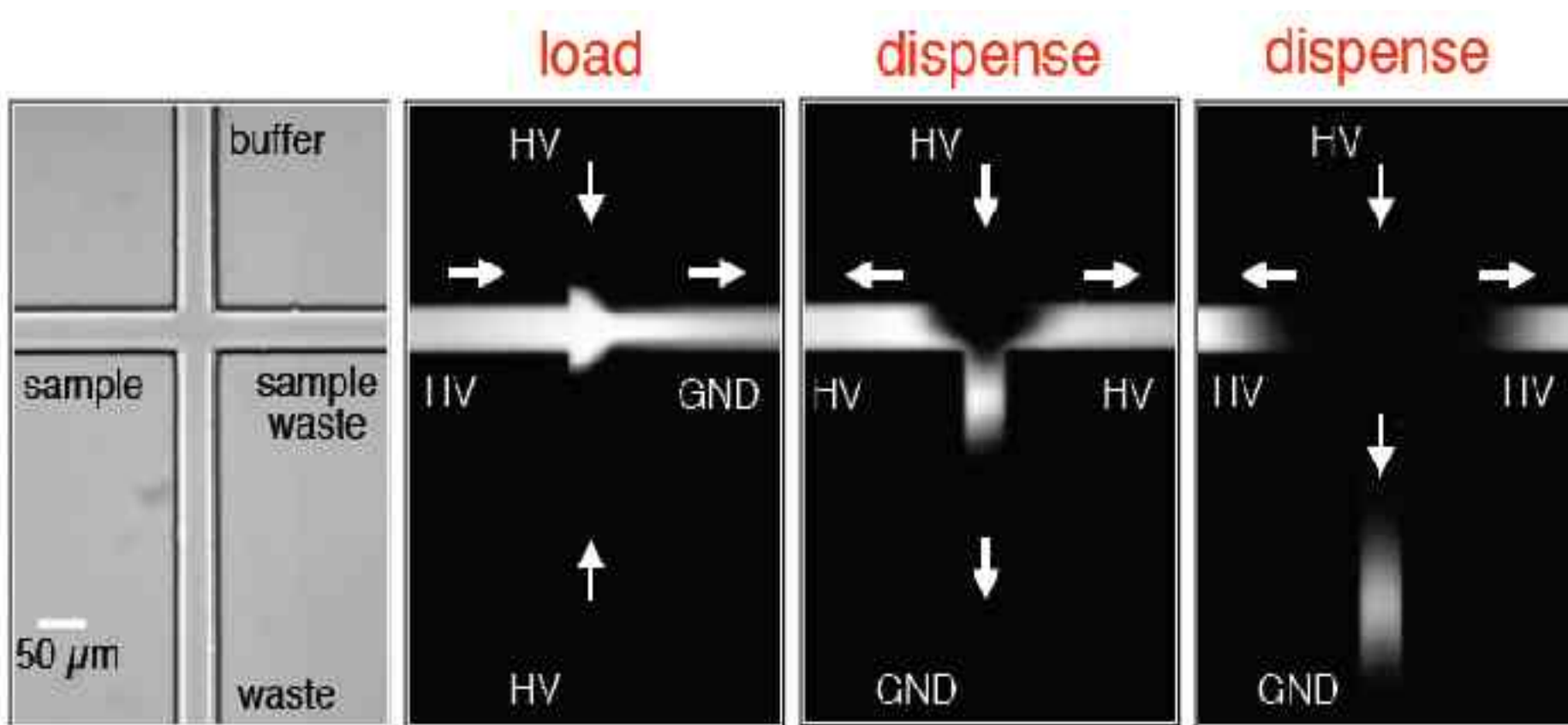


- Negative dielectrophoresis
- Positive dielectrophoresis
- Brownian motion, dielectrophoretic, and electro-osmotic balance



Negative dielectrophoretic force arises when  $\epsilon_{\text{real}}$  becomes negative

# Constant Volume (Pinched Valve)



# Functional Elements

I/O

pipette  
inkjet  
electrospray

separations

electrophoretic  
chromatographic  
sizing  
heterogeneous

filters

physical  
polymeric  
SPE

cytometry

immunoassay  
staining  
cell sorting

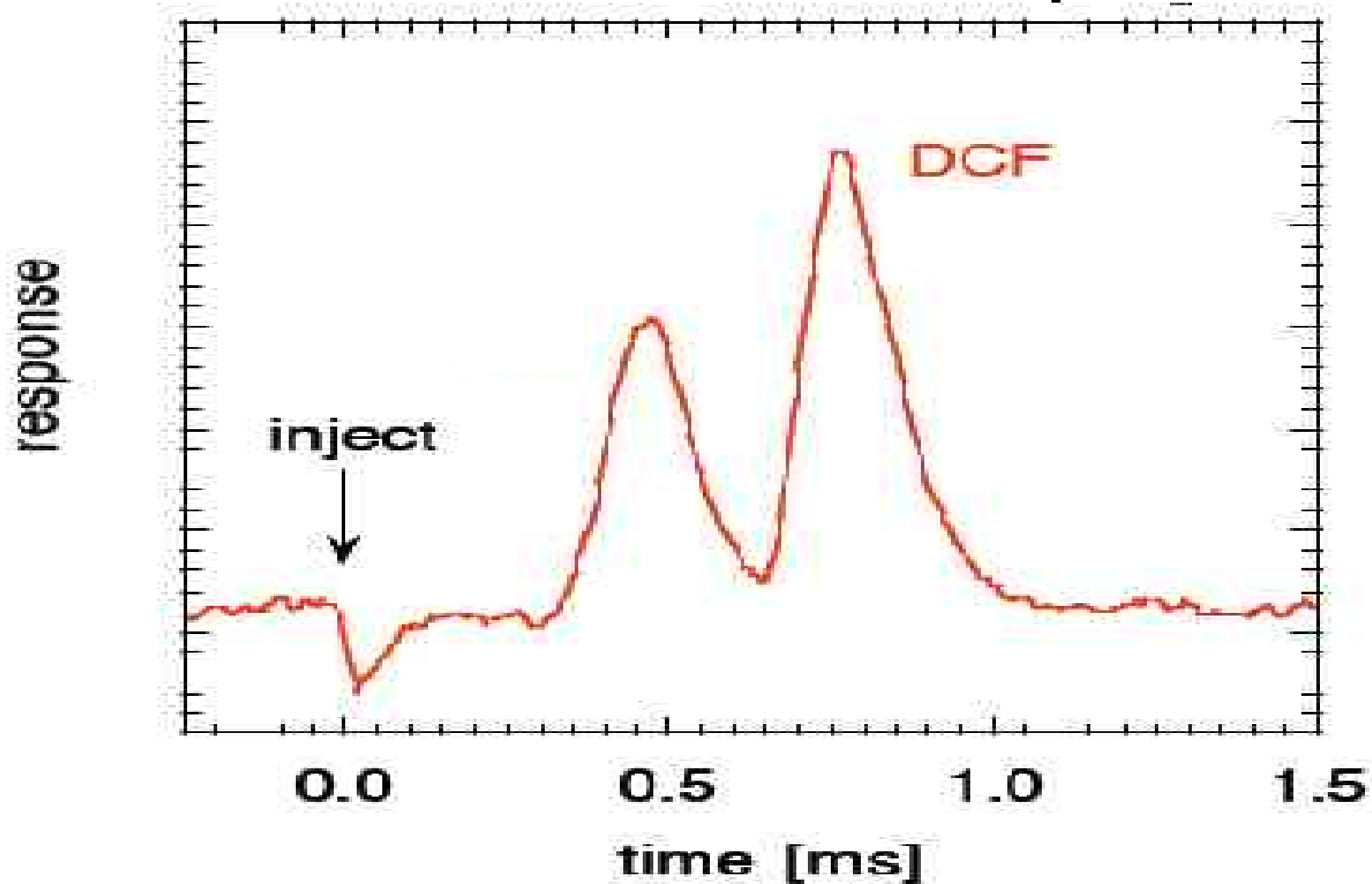
reactions

stopped flow  
continuous flow  
thermal cycling

detection

fluorescence  
absorbance  
refractive index  
scattering  
electrochemical  
MS

# Sub-Milisecond Electrophoresis

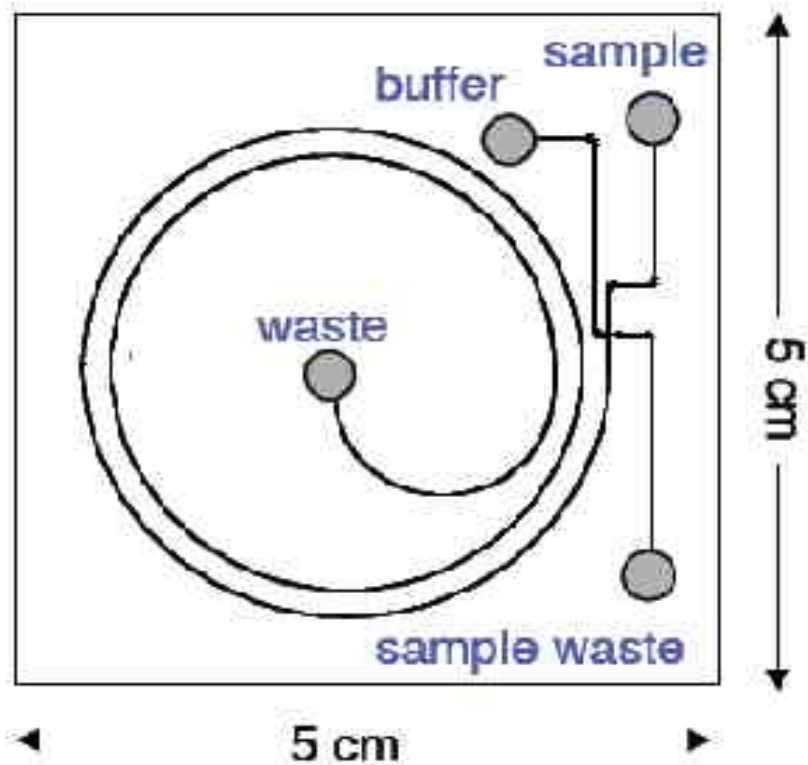


$$L_{\text{sep}} = 200 \mu\text{m}$$

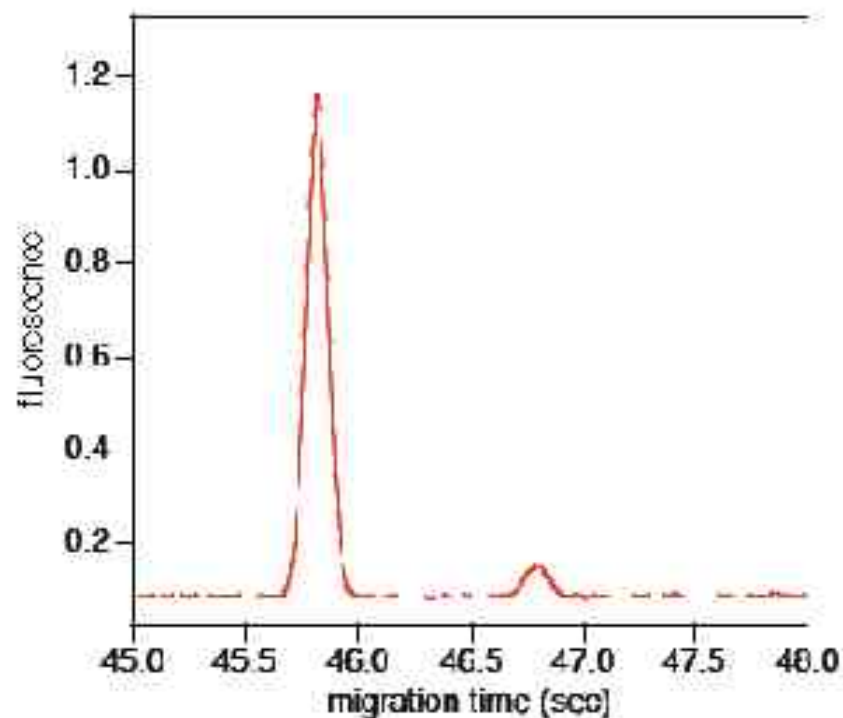
$$E_{\text{sep}} = 53 \text{ kV/cm}$$

*Anal. Chem.*, 70, 3476 (1998)

# Very High Efficiency Separation



$L = 25 \text{ cm}$



Dichlorofluorescein

$N = 1,100,000$

$L_D = 22.2 \text{ cm}$

$E_{\text{sep}} = 1360 \text{ V/cm}$

Buffer: 20 mM Boric Acid  
/100 mM TRIS (pH 9.2)



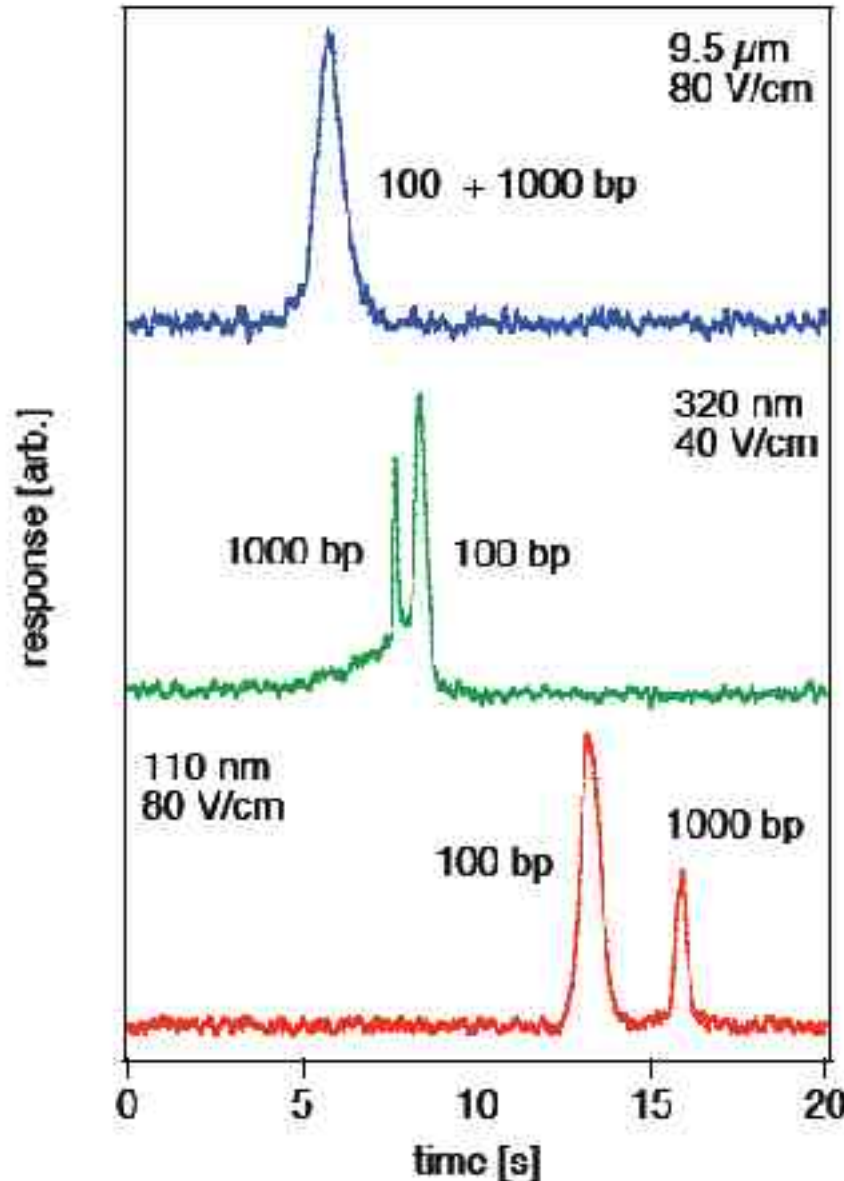
# **Electrokinetically Actuated Segmented Flow**

**Field Free  
Pumping  
of  
Segmented  
Flow**

# Nanofluidics will be Enabling

- **Emulation and interface to biological systems**
  - **Artificial cells**
    - **Biological and chemical sensing**
- **Molecular characterization**
  - **Molecular counting**
  - **DNA sequencing**
  - **Protein and peptide sizing**
- **Fabrication (synthesis) of single molecules**
  - **Heterogeneous polymers**
  - **Complexes with controlled substitution**
- **Hardened (self-repairing) electronics**
  - **Fluidic-based molecular electronic gates**
  - **Molecular-based memories**

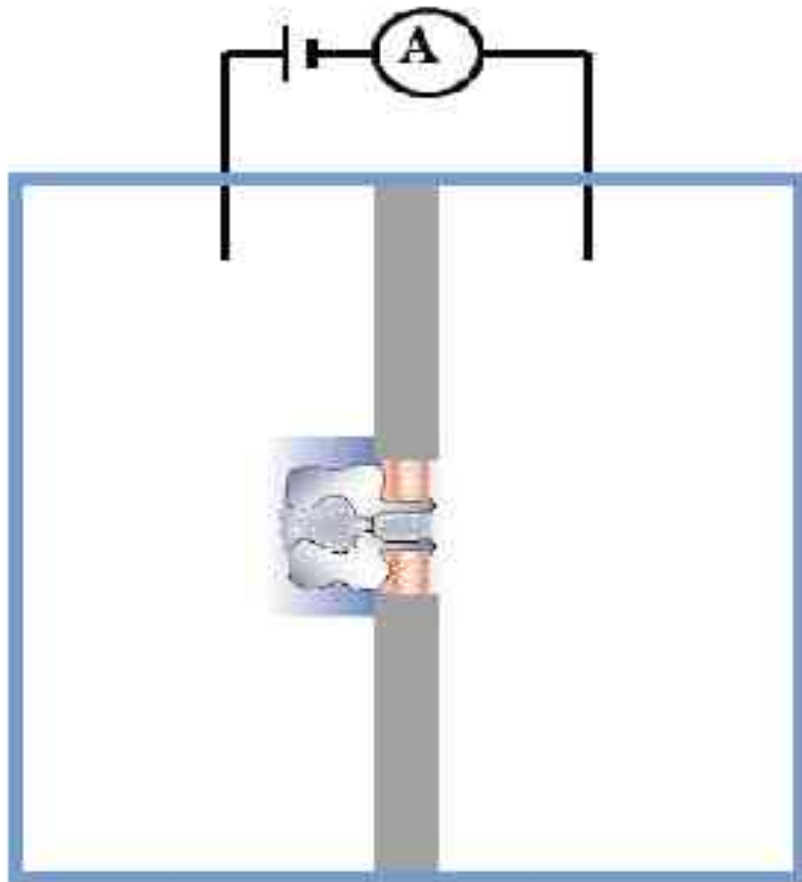
# Electro Hydrodynamic Separation of DNA



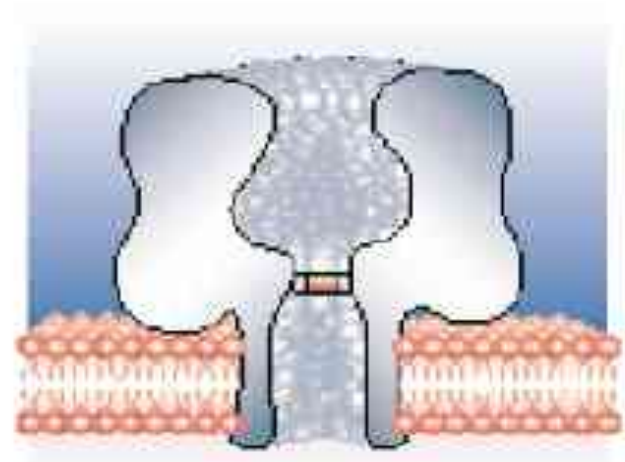
radius of gyration  
25 nm (100 bp)  
75 nm (1000 bp)

$$R_g \approx h$$

# Stochastic Chemical Sensing with Ligand Gated Ion Channels

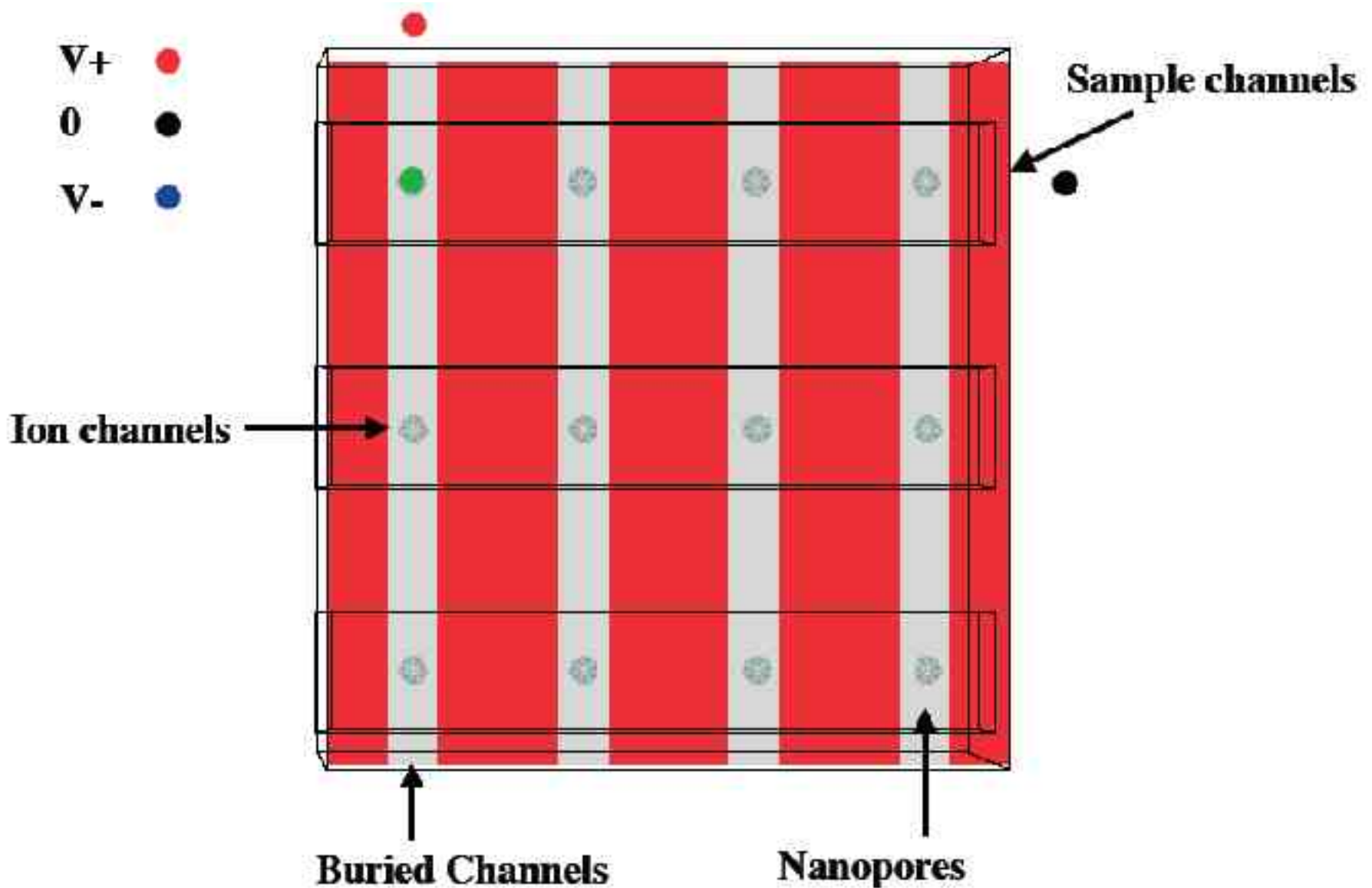


**Planar Lipid Bilayer Apparatus**



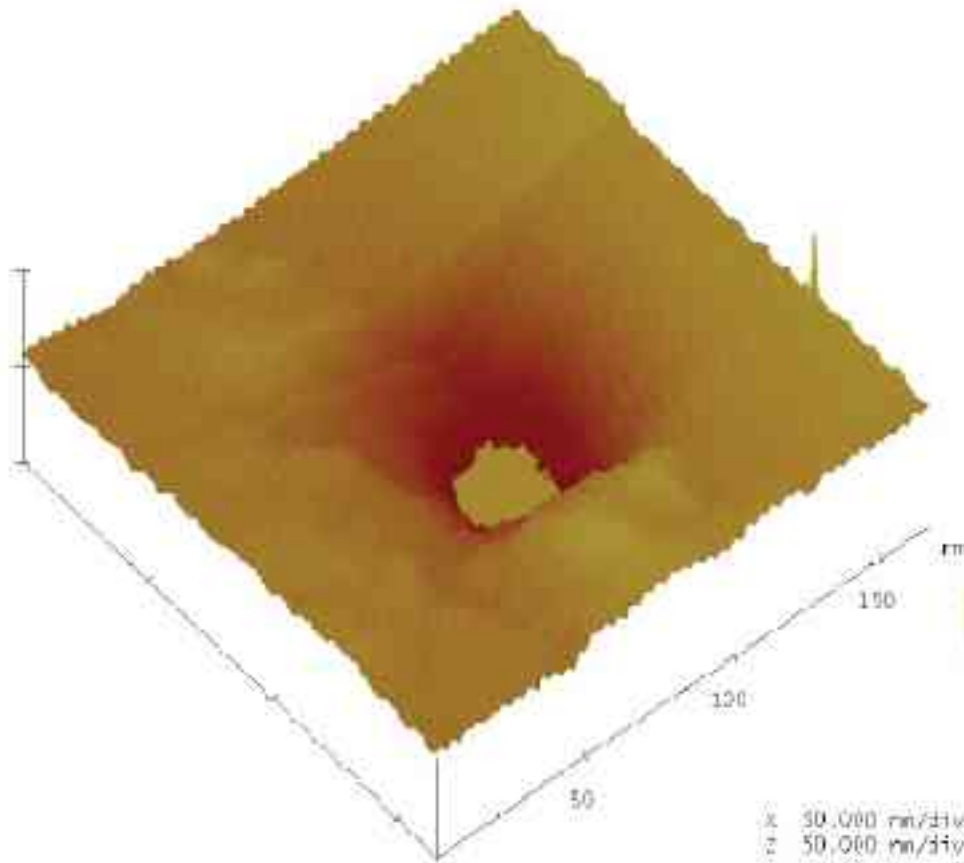
H. Bayley, P. S. Cremer, *Nature*, 413, 226 (2001).

# Addressable Ion Channel Arrays

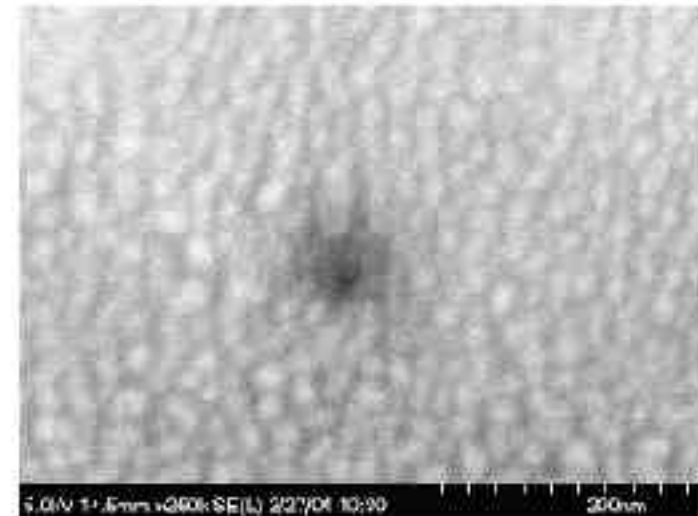


# FIB Milled Nanochannels in SiO<sub>2</sub> Membranes

- 40-nm thick SiO<sub>2</sub> membrane
- 500  $\mu$ S FIB dwell time, 70 pA
- AFM tip:  $r = 40$  nm;  $\theta_{1/2} = 35^\circ$
- Estimated diameter  $\approx 50$  nm



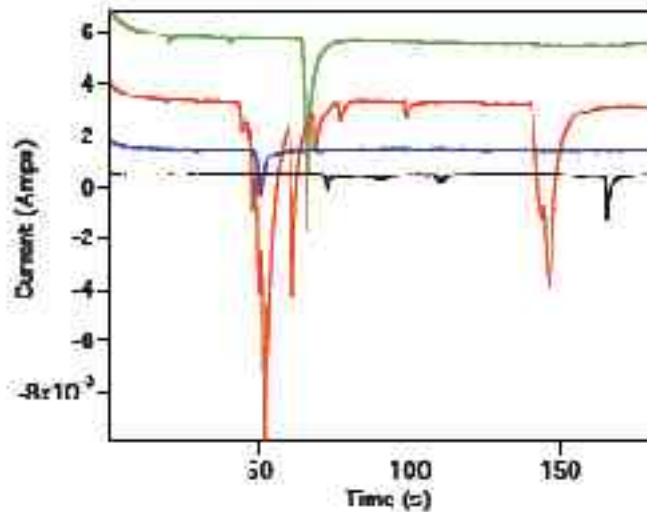
**AFM Image**



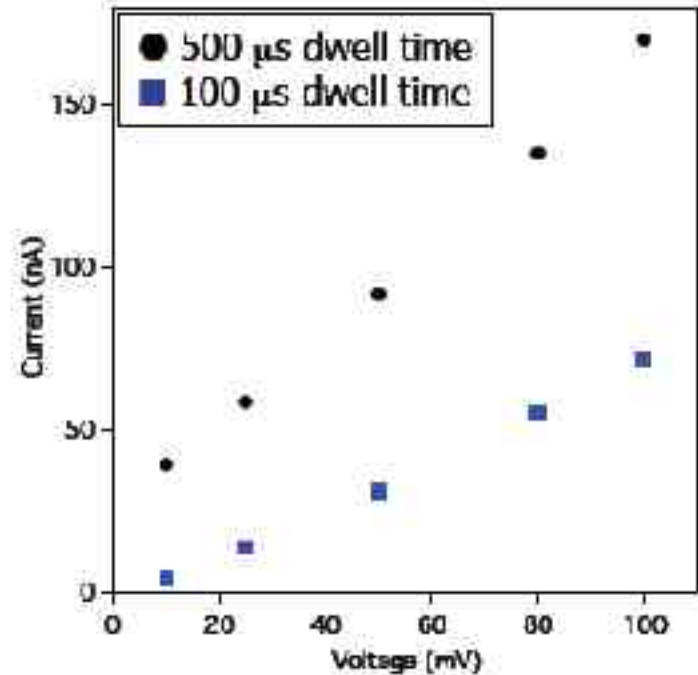
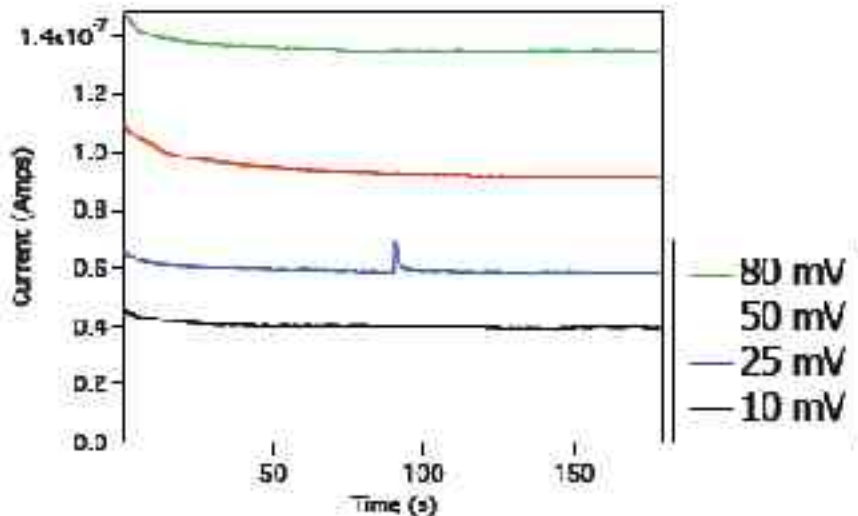
**SEM Image**

# Conductance Measurements

100  $\mu$ S dwell time



500  $\mu$ S dwell time



Electrolyte: 1 M KCl